



MAGNETIC RESONANCE IMAGING (MRI) POWERFUL TOOL TO EXPLORE THE BRAIN

<u>1937 Rabi (Nobel Prize 1944)</u> - resonance method for recording magnetic properties of atomic nuclei
 1940 Zavoyski – discovery of electron paramagnetic resonance
 <u>1946 Block, Purcell (Nobel Prize 1952)</u> – developments of new methods for nuclear magnetic precision
 measurements, and related discoveries
 <u>1973 Lauterbur (Nobel Prize 2003)</u> – First MR images on samples
 <u>1977 Mansfield (Nobel Prize 2003)</u> – First clinical MR images

- NMR measures magnetization of atomic nuclei in the presence of external B₀ magnetic field
- Particles with mass (proton) spin on their axis at Larmor frequency
- Signals are obtained from the NMR observation of proton in body water





Larmor frequency ($\omega > \gamma Bo$)

 ω is the precession frequency (Hz)

 γ is the gyromagnetic ratio

Spin precession around Bo direction

"Why NMR and MRI Need Ultra-high Field Superconducting Magnets: A Biomedical Research Perspective"

Joanna Long, University of Florida, National High Magnetic Field Laboratory

Plenary Session Tuesday, November 3rd 3:45 pm-4:45 pm



MEDICAL IMAGING AND NEURO-IMAGING

One of the best tool to study the human brain













Health

- Neurology / Neurosurgery
- Development, aging, rehabilitation surgery
- Psychiatry, mental disorders

Neurosciences ... structures & functions of the brain



Interaction, society

- Social behavior and culture, art, ..
- Human-Computer Interaction
- Learning, education, ...



IN RECENT DECADES NEUROSCIENCE MADE EXTRAORDINARY PROGRESS





SNR GAIN \propto B0 : CLINICAL RESEARCH APPLICATIONS

Example of a human hippocampus image - Courtesy Neurospin/CEA



Pohmann et al. Magn Reson Med 2016;75:801–809



1 to 2 mm resolution 0.5 to 0.3 mm resolution 0.1 to 0.2 mm resolution

At the ultra-high spatial resolution provided by 7T and soon 11.7T MRI :

 $\Rightarrow\,$ High accuracy segmentation of the hippocampus becomes possible!

 \Rightarrow Highy interesting information for clinical research : Alzheimer's Disease, epilepsy, schizophrenia ...





SNR GAIN AND FUNCTIONNAL SENSITIVITY \propto B0 : NEUROSCIENCE APPLICATIONS



Zoom on the cortical layers



Cortical layers observed in histology



Anatomical 7T MRI (T2*)

> 7T functional MRI: 800 μm isotropic



Voxel distribution over the three gray matter layers.

Selective Activation of the Deep Layers of the Human Primary Visual Cortex by Top-Down Feedbacks. Kok et al. Current Biology 2016

At 7T: first cortical layer-specific cognitive studies, at 11.7T : towards 500 μm isotropic fMRI ...



EARLY NMR IMAGING MAGNETS 1977 - 1981





1978 Philips 0.15T MR scanner
1979 Siemens 0.2T MR scanner
1981 Superconducting MRI scanners (0.5 T, Oxford)
1983 GE generates images with 1.5T scanner

Aberdeen 0.03T resistive magnet - 1977



0.15T Resistive magnet - 1980



John Woodgate and the first 0.3T NMR Imaging Magnet for EMI



First 1.5T magnet (STAR)

Courtesy G. Gilgrass



FAST EVOLUTION OF MAGNET DESIGN 1982 - 2005

1986 Actively-shielded superconducting scanners
1991 fMRI invented – (15 yrs after first clinical images)
1993 Philips: Compact, actively shielded, no LN shield scanners
1994 Diffusion Tensor Imaging invented
1997 GE introduces ZBO scanners: no LHe refill over lifetime
2000 Commercial 3 T MRI from GE, Siemens and Philips
2001 GE, Philips: High-field Open MRI systems
2005 Siemens: wide-bore cylindrical scanners (70-cm patient bore)

2015 100 million MRI scans per year



2015: 7 Tesla Active Shield *First clinical (FDA approved) system – first installations:*

- University of Erlangen, Germany
- Cambridge University, UK.



Courtesy G. Gilgrass



EXAMPLES OF EXISTING ULTRA HIGH FIELD MRI MAGNETS



9.4 T 90 cm 54 tons MRI PET Scanner in operation at Julich, Germany



11.7 T 68 cm MRI Passively Shielded Head Scanner to be commissioned, NIH Clinical Center, Bethesda, USA – Gachon Medical University, Seoul, Korea



10.5 T 88 cm Passively Shielded in operation, CMRR, Minneapolis, USA

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Size

Superconductor

Cold structure

Warm structure

Whole system

DP weigth

ISEULT 11.7 T MRI WHOLE BODY MAGNET AN IDEA IN 2001...

The original idea

Pr. Denis Le Bihan CEA Neurospin

A very preliminary magnet concept a few years later... July 2004

232kg (for main coils)

38t

48t

153t

Length 5m, Diameter 4m

64t (47t main coils, 17t compensation)

The initial specification

B₀ Useful bore Homogeneity Ø10cm Stability 10 gauss line inside magnet room

11.7436T 900mm <0.1ppm 0.05ppm/h



ISEULT Understand the Human Emotions



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ISEULT PROJECT- A FRENCH GERMAN INITIATIVE

French-German industrial collaboration developing : "Molecular Imaging at Ultra High Magnetic Fields"

Agreement signed between Président Jacques Chirac and Chancellor Gerhard Schröder in 2004.

Funding agreement for the French Consortium validated by the French Industrial Innovation Agency in 2006.

Leader of French Consortium : Pharmaceutical Company Guerbet



3 Workpackages

- Development of an ultra high field MRI system (11.7T)
- Develop a new generation of gradient system
- Develop a new generation of contrast media





ISEULT PROJECT - SCIENTIFIC GOALS



Post-mortem inference of the human hippocampal connectivity at 11.7T. J. Beaujoin, C. Poupon et al. *Brain Structure and Function, 2018.*

Study the brain anatomy and connectivity at unprecedented spatial resolution

Explore brain function and metabolism using new contrast mechanisms

Identify new biomarkers for the diagnosis or monitoring of neurological and psychiatric disorders



Effects of anesthetic agents on brain blood oxygenation level at 17.2T. L. Ciobanu, D. Le Bihan et al. *PLoSOne, 2012.*

Exploration of the brain at the mesoscopic scale :

- Non-invasive imaging
- > Whole human brain
- In vivo



Ultra High Field MRI :

- Signal increase
- New contrasts
- \Rightarrow New discoveries



QUEST FOR HIGH FIELD MAGNETS IN FRANCE FROM PHYSICS TO MEDICAL APPLICATIONS

LHC Experiments

1990s

ATLAS Barrel Tor

1980s

40 Years of History of Large SC Magnets

CMS Solenoid





LNCMI 8 T Solenoid

2000-2010s MRI



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THE ISEULT MAGNET

A challenging specification:

- B0 / Aperture 11.75T / 900mm
- Field stability 0.05 ppm/h
- Homogeneity < 0.5 ppm on 22 cm DSV
- Stray field 5 G 13.5 m axial, 10.5 m radial

Innovative solutions for a MRI magnet

- 170 NbTi double pancakes for the main coil
- **2 NbTi shielding coils** to reduce the fringe field
- Cryostat for **superfluid helium at 1.8 K**, 1.25 bars
- Dedicated cryorefrigerator (70 l/h + 40 W @ 4.2 K)
- Driven mode operation with two 1500 A power supplies

Stored Energy	338 MJ
Inductance	308 H
Current	1483 A
Length	5.2 m
Diameter	5 m
Weight	132 t



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WINDINGS & CRYOSTABILITY

- Specific design for the Main Coil made of «Wetted» Double-Pancakes using Non-Insulated Conductor to ensure the • **Cryostability** Inter-turn Inter-pancake
- Shielding Coils are vacuum impregnated with epoxy resin •







ISEULT HELIUM VESSEL ASSEMBLY PRINCIPLE

One key concept is that the main coil is **only mechanical linked to the helium vessel by its extremities** with spring washers and without any inner mandrel or outer support cylinder.



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ELECTRICAL SYSTEM FOR DRIVEN MODE OPERATIONS

The quench protection scheme and the risk of developing superconducting joint using multi-strand cable required the need of a driven mode scheme for the power supply.

But the *specification of +/- 0,05 ppm/h* cannot be reach with a stabilized power supply (max. 1 ppm/h).

=> <u>New concept to stabilize the magnetic field for Iseult</u>

Fault current limiter (FCL) and filtering resistance in parallel with the magnet and the power supply



Current stability on prototype magnet H0 (1.5 T, 900 A, 1H):



Iseult electrical diagram

Fault current limiter (FCL) in series with a filtering resistance *Rf,* in parallel with the magnet

CEA Patent WO/2009/063150



A RELIABLE SYSTEM FOR 24 HOURS SAFE OPERATIONS

Active Quench Protection

through voltage detection and external dump resistor

Maximum terminal voltage:	3600V
Hot Spot temperature (MC):	120K
Hot Spot temperature (SC):	150K

High availability

Redundancy of all key equipment

Two power supplies

48V batteries in case of power failure

Building equipped with a diesel generator





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GENERAL SCHEME OF THE CRYOGENIC EQUIPMENT



Make the magnet and cryogenics «independents» Use reliable technologies and redundancy of equipment Continuous operation in case of failure of cryoequipment



STRONG R&D AND PROTOTYPING ACTIVITIES 2006-2009



Conductors, winding techniques, mechanics, cryogenics, thermo-hydraulic studies...

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CONDUCTORS

160 km of main coil conductor: 1500 A at 11.7 T and 2.8 K, 9.2 mm x 4.9 mm

60 km of shielding coil conductor: 2100 A at 5T, 1.8 K , 9.1 mm x 4.2 mm

R&D Alstom/CEA



Manufactured by Luvata Waterbury, CT, USA,



- •Critical current above the specification +10 %
- •No cabling degradation
- •Good dimensional reproducibility +/- 15 μ m
- Yield strength > 250 MPa



Main coil conductor : Rutherford cable with 10 Cu/NbTi strands in a copper channel using SnSb solder



Shielding coil conductor: Cu/NbTi strand in a copper channel



MAGNET MAMUFACTURING (2010 – 2017) DOUBLE PANCAKE WINDING TECHNIQUE

170 DP wound and controlled (external diameter of 2 m)

- 330 kg each
- Tolerance at inner bore +/-0.05mm
- Control of each turn +/-0.2mm
- Planarity 0.1mm
- Parallelism 0.2mm













Main coil - DP stacking

MAGNET MANUFACTURING (2010 – 2017)



Shielding coil fabrication



MLI wrapping



Main coil / Shielding coils integration



Vacuum vessel welding Wednesday October 28, 2020

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2 WEEKS OF TRANSPORT FROM BELFORT TO SACLAY – MAY 2017





MAGNET CONNECTION TO CRYOPLANT- OCT. 2017 – OCT. 2018

Connection of cryogenic circuits, electrical connection of superconductors and of the inner magnet instrumentation : voltage taps (20), cryoshims (96), quench heaters (8), temperature sensors (96), strain gauges (24)



Circuits assembly





Vacuum vessel welding



Final leak tests (inner cooling circuits and vacuum vessel) Leak rate of 5.10⁻⁹ mbar.l/s on all the internal cooling circuits

MLI

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COOLDOWN - 19 Nov. 2018 - 7 MARCH 2019

- Huge mass to cool down: cold mass (105 tons @ 1.8K) + thermal shield (3.4 tons @ 55K)
- Cooling rate limited by the thermal gradients across the coils (50K max)





CRYOGENIC BUDGET

	Measured values
Liquefier parameters	900W @ 55K (transfer lignes + satellite)
	40W @ 4.5K
	72 l/h @1.8K



ltem	Estimated	Measured
Magnet thermal shield @ 55K	570 W	572 W
Satellite + transfer lines @ 4.5K	27 W	16 W (*)
Cold mass (magnet + current leads) @ 1.8K	35 l/h	17 l/h

(*) without the transfer lines (they are too difficult to measure accurately)

The cryoplant should be able to handle safely the additional thermal losses deposited when all the imaging system is in operation (especially during the gradient coil sequences in DC mode).

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STEP BY STEP ENERGIZATION 11.72T – MARCH - JULY 18TH 2019





FIELD HOMOGENEITY MEASUREMENTS



e New field camera 499MHz developed by Metrolab

- 40 NMR probes
- 50 cm diameter

	300K	1.8K 1.5T	1.8К ЗТ	1.8К 7Т	1.8K 11.7T	Cryoshim power
Z ₁ [ppm]	-132	-16	-7	-5	9	+/- 300
Z ₂ [ppm]	-105	-22	-16	-15	-17	+/- 70
Z ₃ [ppm]	20	2	2	2	2	+/- 10
X ₁ ¹ [ppm]	-1	22	21	22	24	+/- 32
Y ₁ ¹ [ppm]	59	63	59	60	62	+/- 32
X ₂ ¹ [ppm]	-	2	2	2	2	+/- 14
Y ₂ ¹ [ppm]	-	-6	-6	-6	-7	+/- 14
X ₂ ² [ppm]	-	-1	-1	0	-1	+/- 10
Y ₂ ² [ppm]	-	0	-1	-1	-1	+/- 10



• Very good agreement between the measurements (1.5T, 3T, 7T, 11.7T)

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PASSIVE SHIMMING AT 3 T AND 7 T (JUN – JUL. 2020)

- Implementation of the additional iron shims
- Optimization of shim pattern (27kg of iron)
- Assembly of the 72 rails (41 aluminium/iron parts per rail)
- Magnetic measurements at 3T and 7T
 - Validation of the homogenization method and the additional shim effect; several more iterations will be needed to reach the 0.5ppm spec





- **Confirmation at 7T of the 3 T results** (slight variations due to disassembly
- / reassembly of the bench between the two measurements)
- Final adjustment to be made after setting up the gradient.

DHS		3T	7T
	11,7T w/o iron	measurements	measurements
		extrapolated at	extrapolated at
		11,7T	11,7T
		with iron	with iron
Z ₀ [T]	11,7	11,7	11,7
Z ₁ [ppm]	-5,6	0,2	11,9
Z ₂ [ppm]	-16,9	0	-1
Z ₃ [ppm]	3,6	0,1	-0,8
Z ₄ [ppm]	1,3	1,3	1,5
Z ₅ [ppm]	-0,1	-0,1	-0,1
X ₁ ¹ [ppm]	23,2	0,8	-2,9
Y ₁ ¹ [ppm]	64,5	-0,4	2,5
X ₂ ¹ [ppm]	2,6	-0,4	0,5
Y ₂ ¹ [ppm]	-7,1	-0,1	-0,1
X_2^2 [ppm]	-0,6	-0,4	-0,6
Y_2^2 [ppm]	-1,2	-0,5	-0,4

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MRI System Equipment (Oct. 2019 – Oct. 2020)

- \circ Covers
- $\circ~$ Room walls
- $\circ~$ Patient bed
- Faraday cages
- $\circ~$ Gradient coils
- $\circ~$ Consoles









FINAL COMMISSIONING STEPS OF THE ISEULT MRI SYSTEM AND FIRST IMAGE IN 2021

- Installation of the MRI equipment (Gradient Coils, RF antenna, ...)
- Final commissioning steps until mid-2021 :
 - Final commissioning of the high-availability control and protection systems
 - Final adjustment of the field homogeneity (iron shims cryoshims)
 - Final adjustment of the field stability
 - Tests of the impact of the gradient coil operations on magnet operations (He consumption, eddy currents etc..



Brain image at 7T (courtesy of Neurospin)

After 20 yearsthe start of a new adventure



PERSPECTIVES FOR THE FUTURE



International collaborations with academics and industries to develop MRI magnets for the future

Rendezvous in 20 years!

